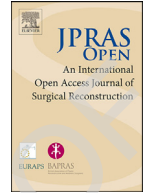




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Review Article

History of breast implants: Back to the future

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ABSTRACT

Modern breast implants are a staple of plastic surgery, finding uses in esthetic and reconstructive procedures. Their history began in the 1960s, with the first generation of smooth devices with thick silicone elastomer, thick silicone gel, and Dacron patches on the back. They presented hard consistency, high capsular contracture rates and the patches increased the risk of rupture. In the same decade, polyurethane coating of implants was implemented. A second generation was introduced in the 1970s with a thinner shell, less viscous gel filler and no patches, but increased silicone bleed-through and rupture rates. The third generation, in the early 1980s, featured implants with a thicker multilayered elastomer shell reinforced with silica to reduce rupture risk and prevent silicone bleed-through. A fourth generation from the late 1980s combined thick outer elastomer shells, more cohesive gel filler, and implemented for the first-time outer shell texturing. In the early 1990s, the fifth generation of devices pioneered an anatomical shape with highly cohesive form-stable gel filler and a rough outer shell surface. Surface texturing was hampered by the discovery of Breast Implant Associated-Anaplastic Large Cell Lymphoma and its link with textured devices. From the 2010s, we have the era of the sixth generation of implants, featuring innovations regarding the surface, with biomimetic surfaces, more resistant shells and variations in gel consistency. The road to innovation comprises setbacks such as

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the FDA moratorium in 1992, the PIP scandal, the Silimed CE mark temporary suspension and the FDA-requested voluntary recall of the Allergan BIOCELL implants.

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1 Introduction

2 The term “breast implant” (BI) refers to any implantable prosthesis used to modify or replace a
3 person’s breast contour, shape and size. Despite the great variability, they can be grouped according
4 to three characteristics: fill, shell surface and three-dimensional shape.

5 In the European and American markets, they are most frequently filled with silicone gels of varying
6 levels of cohesiveness, resulting in different viscosity and firmness. The second most commonly used
7 filler material is saline solution. Less commonly used fillers include methylcellulose, soybean oil and
8 others. All shells are made of silicone and fabricated by adding different layers (3–5) on top of each
9 other to increase their strength against rupture or become impermeable to silicone, hindering bleed-
10 through.

11 The external surface of the shell can have different aspect with different degrees of roughness,
12 ranging from a non-perceptible one by touch (smooth), to a shallow or deep texturing, or it may also
13 be coated with polyurethane (PU).¹

14 Based on the above, several classifications mainly based on physical properties have been proposed.
15 Barr et al. divided BIs according to surface roughness in Nano (<5 µm), Meso (<15 µm), Micro (10–
16 75 µm), and Macro (>75 µm).² Although Atlan et al. used measurements of surface area to classify
17 implants into Smooth (80–100 mm²), Micro (80–100 mm²), Macro (200–300 mm²), and +Macro
18 (>300 mm²).³ Jones et al. instead, first introduced the integration of a biologic property as the bac-
19 terial attachment to surface with the physical measurements of roughness, to classify implants into
20 Minimal (<25 µm), Low (25–75 µm), Intermediate (75–100 µm), and High (>150 µm).⁴

21 Today the most widely accepted classification remains the ISO 14607:2018, which divides surfaces
22 based on their average roughness into Smooth (<10 µm), Micro (10–50 µm), and Macro (>50 µm).¹ Nev-
23 ertheless, there is still need for a more comprehensive classification of implants integrating physical
24 properties to their host interaction connected with most of BI complications (capsular contracture,
25 BIA-ALCL).

26 Shape can either be *round*, a lenticular shape, with a symmetrical curved anterior side (dome)
27 and a flat round posterior base; or *anatomical*, a teardrop shape, with the upper half having a lower
28 projection compared to the enhanced projection of the lower half. They have an asymmetric curved
29 anterior side and a flat, more often round or elliptical posterior base. These implants are filled with a
30 highly cohesive gel to maintain their anatomical shape and are rough to prevent their rotation.

31 BIs undoubtedly represent a staple of plastic surgery, finding indications for both esthetic and re-
32 constructive purposes. Their manufacturing has evolved significantly to overcome health concerns all
33 the while accommodating the needs of patients, which is why they have gone through several itera-
34 tions of changes.^{5,6} The aim of this paper was to present a recollection of the main BIs and relative
35 events that paved the way to the development of modern BIs used today in the European and Amer-
36 ican markets, as well as the defining moments that will guide devices of the future.

37 “Prehistory” – the dawn of breast implants

38 The first modern BI was introduced by Thomas Cronin and Frank Gerow in 1962, and the first gen-
39 eration of these devices was commercially produced using silicone by the Dow Corning Corporation,

40 reaching US markets in 1964. They were manufactured with a smooth outer surface, a thick silicone
41 elastomer (~0.75 mm) shell filled with thick viscous polydimethylsiloxane (PDMS) silicone gel (com-
42 posed of a mix of 50% low molecular weight chain [LMWC] components which are more fluid, and
43 50% high molecular weight chain [HMWC] components which are more viscous) and Dacron fixation
44 patches on the posterior aspect to maintain their position.⁷ Later the Dacron patches were deemed
45 dangerous as they created a stress point at which the outer shell could tear,⁸ and the devices were
46 performing too firm with an unnatural feel and a high capsular contracture rate. Soon after, in 1964,
47 saline inflatable implants were developed by Laboratoires Arion,⁹ and because of their softer consistency
48 gained a first wave of popularity in the 1970s as an alternative to Dow Corning BIs. However,
49 they presented many cosmetic disadvantages and a much higher risk of deflation and implant failure,
50 thus their market remained limited to the USA.^{10,11} Natural-Y Surgical Specialties Inc. developed in
51 1964 and made available in 1968, the first type of silicone BI with an irregular sponge-like surface,
52 coated by a 1- to 2 mm-thick layer of PU foam. This feature was intended to enhance tissue integra-
53 tion¹² and counteract capsular contracture which plagued the previous generation of BIs.¹³ Their in-
54 ternal baffle was divided in the shape of a “Y” into 3 compartments, to minimize bulging of one com-
55 partment when another was compressed.¹⁴ In 1970s, silicone gel-filled Dow Corning implants were
56 improved upon with a second generation having a thinner shell (~0.13 mm), no Dacron patches and
57 less viscous, low cohesion silicone gel (containing a mix of 80% LMWC and 20% HMWC).¹⁵ Although
58 these BIs provided a more natural feel, their shell appeared to be permeable to silicone gel and they
59 were subsequently plagued by microscopic bleeding and spreading of silicone droplets mainly to sur-
60 rounding tissues and locoregional lymphonodes. In addition, they were less durable than their prede-
61 cessors and ruptured frequently.^{16,17}

62 Importantly, these concerns and drawbacks, on one hand caused silicone BI regulations to shift
63 in 1976, with the Food and Drug Administration (FDA) subjecting BIs to controls and performance
64 standards with the enactment of the Medical Device Amendments,¹⁸ whereas forced companies for
65 further innovations.

66 In 1976 Heyer-Schulte, in the attempt to overcome the silicone gel bleeding first introduced the
67 “double lumen” BI, consisting of a silicone-filled core enclosed by a saline-filled outer shell.¹⁹ This
68 has paved the way for the introduction of a third generation of BIs in the 1980s, which implemented
69 a thicker multilayered elastomer shell (0.28–0.3 mm) reinforced with silica to reduce implant rupture,
70 prevent gel migration and stop silicone bleed-through. In 1984 Mentor manufactured a “reverse dou-
71 ble lumen” implant also known as the Becker permanent expander, opposite to the previous produced
72 by Heyer-Schulte.²⁰ It consisted of a saline implant connected to a filling tube and a valve encased
73 within a silicone implant, in an attempt to combine the esthetic benefits of silicone gel in the outer
74 lumen with a postoperatively adjustable volume from the inner lumen, particularly advantageous in
75 reconstructive and asymmetry cases.

76 In spite of all the improvements, several reports of adverse events in patient with previous BIs be-
77 gan to appear in the medical literature” in the 1980s, and the FDA decided to designate BIs as class III
78 medical devices with the Federal Register of June 24, 1988 (53 FR 23856): this implied that manufac-
79 turers needed rigorous approval from the FDA proving that their devices were medically safe before
80 they could be sold and marketed.²¹ Unfortunately the regulations arrived a little too late, as patients
81 began suing manufacturing companies, arguing that the implants caused a variety of complications
82 of which they had not been informed prior to surgery, including diseases of the immune system and
83 breast cancer.

84 In the late 1980s, reports emerged also regarding the *in vitro* degradation of PU, which could lead
85 to formation of 2,4-toluenediamine (2,4-TDA), known to be carcinogenic in animals, and raising con-
86 cerns about its potential carcinogenicity in humans.^{22,23} The FDA, after performing a risk analysis,
87 concluded that the lifetime risk of PU-induced cancer in women with a single pair of PU-coated BIs
88 was about 1 in 1000,000. This, according to the WHO definition of “acceptable cancer risk”,²⁴ led the
89 FDA to recommend that women with PU BIs should not have their devices removed based solely on
90 concerns about cancer from 2,4-TDA.²⁵ Although in 1991 the main PU-BI manufacturers Surgitek (sub-
91 sequently Bristol-Myers Squibb) voluntarily withdrew its devices manufactured in the USA, which had
92 been implanted in 110,000 American women by that time,^{26,27} foreign producers continued to man-

93 manufacture PU-coated BIs outside the USA, and these devices have been widely used throughout Europe
94 and other parts of the world in the following years.

95 From late 1980s onwards, the fourth generations of BIs were developed with manufacturing criteria
96 and quality control more stringent and rigorous than ever, due to the legislative FDA changes of 1988.
97 The BIs included thick outer elastomer shells (~0.5 mm), in some cases similar to that of previous
98 generations of BIs, and a cohesive gel filler (manufacturer-specific) which was thought to be less likely
99 to rupture and leak silicone.²⁸ They were most commonly round and with moderate cohesivity gel
100 filler, and began implementing texturing of outer shells with different processes, including “salt-loss”
101 and “imprint stamping” techniques to allow for more integration by tissue ingrowth into the irregular
102 spaces of the shell.

103 In 1990 Mentor licensed barrier technology to McGhan (subsequently Inamed and then Allergan
104 from 2006) which began producing their own line of “double-lumen” devices similar to Heyer-Schult.
105 However, the complex structure of these devices caused higher failure rates than previous BIs, and
106 despite Mentor Becker expanders still being in distribution, double lumen implants began falling out
107 of favor at the turn of the century.²⁹

108 By the early 1990s, Dow Corning was entangled in a litigation counting over 12,000 women who
109 partook in a class-action lawsuit.³⁰ Pressured by media frenzy over BI litigation, the FDA evaluated
110 that evidence supporting the safety and effectiveness of BIs was insufficient, and thus placed a tem-
111 porary moratorium in January 1992, banning the use of silicone BIs in the USA.³¹ In April of the same
112 year, the ban was revoked, but access to silicone BIs was limited to breast reconstruction, correction
113 of congenital deformities and revisional cases. During the moratorium, saline inflatable BIs received
114 some newfound popularity because they became the only option for esthetic breast augmentations in
115 the USA, but never gained much popularity in the rest of the market where moratorium and limita-
116 tion were not imposed.^{32,33} Meanwhile, Dow Corning which was the world’s largest implant manu-
117 facturer of its time, controlling 35% of the market, agreed to pay \$3.2 billion as settlement with the
118 claimants in 1994, but then later filed for bankruptcy in 1995 due to the number of lawsuits it was
119 still facing. This effectively caused the corporate giant to withdraw from the implant market.³⁴ Nev-
120 ertheless, overwhelming research disproved the claims that BIs were linked with breast cancer and
121 connective tissue diseases.^{35,36,37} Although the link with autoimmune and rheumatic diseases is up
122 for debate, scientific evidence at the time failed to show that BIs caused disease, and after in-depth
123 evaluation the FDA lifted the moratorium for good on November 2006, allowing the use of silicone
124 BIs for women over the age of 22.^{38,39} After lifting the moratorium, the FDA assessed results of core
125 studies and approved in the USA only BIs produced by Allergan⁴⁰ and Mentor.⁴¹

126 “Middle ages” – the darkest hour of breast implants

127 A fifth generation of devices was introduced in 1993 with an anatomical teardrop or “gummy bear”
128 shape and highly cohesive form-stable gel filler to maintain it,⁴² combined with a rough outer surface
129 of the shell (texturing) allowing for ingrowth and adherence with host tissues, necessary to stabilize
130 implants in the correct position in the periprosthetic pocket.⁴³

131 Some brands as Allergan (BIOCELL surface), Eurosilicone, GC Aesthetics, Silimed and others, began
132 producing the “salt-loss” texturization either by spraying, by dipping or sprinkling fine salt crystals
133 onto the silicone shell before curing, and supposedly removed afterwards by rinsing with water with-
134 out brushing.^{44,45} This texturization was coarse and somehow different from the one created by other
135 manufacturers as Mentor’s (Siltex surface), generating a finer homogeneous outer texture by a pres-
136 sure imprint-stamping technique.^{46,47}

137 In this period, fear over health concerns linked to silicone favored the development of filler alterna-
138 tives, as the LipoMatrix’s Trilucent BIs, marketed and sold in Europe from 1995 only with pre-clinical
139 safety data. They differed from previous generations of BIs for being filled with soybean oil, thought
140 to be safer compared to PDMS.⁴⁸ Later evidence suggested high early implant rupture rate,⁴⁹ caused
141 by extreme fragility of the implant’s shell which deteriorated causing bleeding of the triglyceride filler,
142 the latter linked to the formation of toxic oxidation products that caused pronounced inflammatory
143 reaction.⁵⁰ The UK’s Medicines and Healthcare products Regulatory Agency (MHRA) additionally found
144 that the degradation of the oil was linked to cancer and birth defects. After adverse reports Trilucent

145 BIs were voluntarily withdrawn in March 1999⁵¹ and in June 2000, the MHRA was recommended to
146 be removed due to the risk of local tissue exposure to toxic compounds.⁵²

147 The Poly Implant Prothèse (PIP) French manufacturer launched in 1991, and began producing in
148 1997, silicone-filled BIs which became popular for their competitive marketing strategy. After the FDA
149 refusing to approve PIP BIs in 2000 because of deviations from good manufacturing practices, the
150 company came under scrutiny from European regulators in March 2010 when the French Agency for
151 the Safety of Health Products (formerly AFSSAPS, now ANSM) performed an inspection of the com-
152 pany's headquarters following numerous reports of early implant rupture. They found evidence of un-
153 approved low-quality industrial-grade silicone gel used during the manufacturing process instead of
154 medical-grade PDMS.⁵³ Consequently, they ordered to suspend the sale of all PIP BIs and their with-
155 drawal from the market,⁵⁴ affecting approximately 400,000 women in 65 countries⁵⁵ from health risks
156 of locoregional⁵⁶ and systemic silicone spread.^{57,58} It ultimately led to PIP filing for bankruptcy and to
157 the arrest of the company's Chief Executive Officer. Germany's Technical Inspection Association (TÜV
158 Rheinland) was among the bodies that certified PIP implants, and was found liable by French judges
159 according to whom TÜV could not have been oblivious to the fraud.⁵⁹ Because of the seriousness of
160 the situation and the high risk of premature rupture, in December 2011 the ANSM recommended all
161 women with PIP BIs to preemptively remove them,⁶⁰ applying the precautionary principle from the
162 *Treaty on the functioning of the European Union*, Art. 191, which should be applied "when a product
163 may have a dangerous effect, identified by a scientific and objective evaluation, if this evaluation does
164 not allow the risk to be determined with sufficient certainty".^{61,62}

165 Silimed, born in Rio de Janeiro in 1978, started production of BIs in 1981 including PU-coated
166 BIs from 1989, and received the CE mark 1998. On September 2015, the German Federal Institute
167 for Drugs and Medical Devices (BfArM) conducted an inspection of the Brazilian company's manufac-
168 turing plant, finding evidence that surfaces of textured and PU-coated implants were contaminated
169 with man-made mineral fibers (MMMFs), potentially carcinogenic to humans. These MMMFs were
170 not found on their smooth devices, and should not be found on any BI surface in general.^{63,64} As
171 a result of this discovery, the MHRA, jointly with European healthcare product regulators of mem-
172 ber states, again followed the precautionary principle and ordered the suspension of CE certificate for
173 all Silimed medical devices.^{59,65} In the same year, health authorities in the Netherlands appointed
174 the Independent Clinical Expert Advisory Group (ICEAG) to investigate whether MMMFs found on
175 Silimed BIs could elevate cancer risk to a level higher than the "acceptable" one.⁶⁶ The authors of
176 the risk analysis warned about important uncertainties and limitations to their estimate, like the in-
177 traperitoneal introduction of fibers in the rat model used for the study, or the larger size of the fibers
178 (median length of ~180µm and diameter of 9µm) found on Silimed implants, which may lead to a
179 lower toxicity if encapsulated or conversely to a higher toxicity due to frustrated phagocytosis and in-
180 creased biopersistence. In fact, macrophages fail to incorporate and remove foreign bodies larger than
181 >30µm, leading to cytokines storm and chronic persistent inflammation.⁶⁷ Based on that analysis, the
182 cancer risk could range from lower (0.442:1000000) to higher (9:1000000) than 1 in 1000000, and it
183 was considered "acceptable" by EU regulatory agencies, similar to previously done by the FDA when
184 studying PU carcinogenicity. The ICEAG concluded that being the risk "very small and around the ac-
185 ceptability limit", that decisions about risk management in patients with potentially contaminated BIs
186 should be made jointly by patients and their treating physicians.

187 The Australian Therapeutic Goods Administration (TGA) followed suit and canceled all Silimed de-
188 vices from their register on November 2016,⁶⁸ and later Loch-Wilkinson et al.,⁶⁹ Collet et al.⁷⁰ and
189 Magnusson et al.⁷¹ showed a carcinogenicity risk for Silimed PU BIs as high as 1 in 2832 implants.
190 Sientra, which is a US-based company that hired Silimed for manufacturing their BIs, voluntarily
191 placed a temporary hold on the sale in the US of all Sientra devices manufactured by Silimed, advising
192 surgeons to discontinue implanting them.⁷² Sientra has now severed ties with Silimed and manufac-
193 tures its own BIs on American soil. Meanwhile, Silimed has addressed the health concerns and has
194 recovered the CE mark, but Silimed products have not been sold in the EU since 2015.⁷³

195 From 2010 onward, companies have attempted to introduce filler innovations such as the Di-
196 agon/Gel 4 (POLYTECH Health & Aesthetics GmbH) which combines 2 different types of silicone gel,
197 softer on the back while firmer in the front, in a textured anatomical implant.⁷⁴

198 Recently, all textured 4th and 5th BIs become potentially afflicted by another crisis, related to the
199 onset of a hematological cancer named Breast Implant-Associated Anaplastic Large Cell Lymphoma
200 (BIA-ALCL). First reported in 1997 by Keech and Creech,⁷⁵ it was highlighted later by the FDA alert in
201 2011,⁷⁶ and finally recognized as a separate nosological entity by the World Health Organization in
202 2016.⁷⁷ In 2017, the European Commission on Health (DG SANTE) requested the Scientific Committee
203 on Health, Environmental and Emerging Risks (SCHEER) to provide a scientific opinion on the safety
204 of BIs, which concluded that there were “insufficient scientific information available to establish a
205 methodologic robust risk assessment regarding a possible association between BI and ALCL develop-
206 ment” and recommended the scientific community to conduct a more in-depth evaluation.⁷⁸

207 On December 14th, 2018, French notified body GMED denied the renewal of the CE mark for Al-
208 lergan BIOCELL textured BIs and tissue expanders.⁷⁹ This hindered the sale of Allergan BIs across Eu-
209 rope, and was followed soon after by the ANSM’s ban on the sale and use of macrot textured and
210 polyurethane-coated BIs in France on April 4th, 2019, affecting several brands.⁸⁰ FDA followed suit on
211 July 24, 2019, ordering a class I voluntary recall of all Allergan textured devices from the market due
212 to BIA-ALCL risk.⁸¹

213 In 2019, the European Commission on Health (DG SANTE) requested again the SCHEER to provide
214 a scientific opinion on the safety of BIs.⁸² Two years after the previous request it was concluded that
215 there is a causal relationship between all textured BIs and BIA-ALCL, that not all devices give rise to
216 the disease, and that the incidence is higher in patients with macrot textured devices according to ISO-
217 14607:2018, being disproportionately higher with specific types or brands (Allergan Biocell, Silimed
218 Polyurethane).^{67,68} In addition, there is evidence to suggest that this form of ALCL is not only linked
219 to not just BIs, but to implantable textured devices in general.⁸³

220 The scientific evidence for causal relationship was weighted as “*moderate*”, as there are sufficient
221 scientific data from a primary line of evidence, based on a majority of epidemiological studies, that
222 being retrospective case-control studies have limited ability for causal inference. Thus the claim for a
223 causal relationship needs to be strengthened by a secondary etiopathogenetic line of evidence. While
224 accounting for a possible genetic predisposition, the pathogenic mechanism of chronic inflammation
225 leading to lymphomagenesis could be triggered by multiple, possibly combined, etiologic hypotheses
226 such as bacterial contamination, shell shedding of particulates, shell surface characteristics leading to
227 friction, or by implant-associated reactive compounds.⁸⁴ Nevertheless, because of the etiology gaps in
228 the secondary line, reaching a *strong* weight of evidence would require randomized controlled trials on
229 humans, which are obviously unethical and unachievable as high-risk devices have been withdrawn.⁸⁵
230 As most authorities are not giving precise guidance, some surgeons continue using macrot textured de-
231 vices that are still available on the market.^{86,87} Others have abandoned textured BIs altogether, im-
232 plementing the use of smooth devices in their practice instead,⁸⁸ or even evaluating the pre-emptive
233 explantation and replacement from textured to smooth devices.^{89,90} Regardless of personal beliefs, BI
234 markets have responded to the health crisis related to texturing by progressively shifting to smooth
235 implants in some parts of the world.⁹¹ In USA, the use of textured BIs for all placements which started
236 at 3.4% in 2007, increased significantly and peaked at 22.89% in 2016, and then dropped again to 3.61%
237 in 2019.⁹² But with the exception of France, the same cannot be said for other European countries,
238 where textured BIs still represent the majority of used devices until 2018.⁹³ There is no doubt that
239 previous banning, cultural and market differences have created a population of surgeons that are more
240 comfortable using smooth implants in the USA,⁹⁴ compared to their European counterpart, for whom
241 a transition from textured shaped to round smooth devices might jeopardize esthetic outcomes,⁸⁴ and
242 might require a learning curve before achieving similar results.⁸⁵

243 “Modern times” – out with the old, in with the new

244 Necessity is the mother of invention. Today’s most feared macrot textured implant-related compli-
245 cations have been linked to the potential effects of chronic inflammation.⁹⁵ Studies on animal models
246 confirm this by reporting highest amounts of inflammation and foreign body response in devices with
247 roughness >80 μm .⁹⁶

248 This has pushed for the creation of safer BIs with a new sixth generation, which was introduced
249 in the early 2010s and implements evidence-based modifications that help mitigate foreign body re-

Table 1

Silicone breast implant characteristics. Adapted from Barr et al.'s Table "Implant characteristics" (Barr S, Bayat A. Breast implant surface development: perspectives on development and manufacture. *Aesthet Surg J*. 2011;31(1):56–67. doi:[10.1177/1090820X10390921](https://doi.org/10.1177/1090820X10390921)).

Type of BI	Period of Use	Outer Surface	Core	Shell
First Generation	1963–1973	<ul style="list-style-type: none"> - Smooth (< 1 μm) - Dacron patches posteriorly 	<ul style="list-style-type: none"> - Thick silicone - 50% LMWC - 50% HMWC 	<ul style="list-style-type: none"> - ~0.75 mm
Second Generation	1972–1982	<ul style="list-style-type: none"> - Smooth (< 1 μm) 	<ul style="list-style-type: none"> - Thin silicone - 80% LMWC - 20% HMWC 	<ul style="list-style-type: none"> - ~ 0.13 mm - High bleed-through rate
Third Generation	1982 onward	<ul style="list-style-type: none"> - Smooth (< 1 μm) 	<ul style="list-style-type: none"> - Thick silicone 	<ul style="list-style-type: none"> - Early shell: 0.28–0.3 mm - Later shells: dependent on manufacturer - Reinforced with silica
Fourth Generation	1987 onward	<ul style="list-style-type: none"> - Textured (> 80 μm) - with salt-loss or imprint molding technique 	<ul style="list-style-type: none"> - Manufacturer-specific - Generally moderate cohesive silicone 	<ul style="list-style-type: none"> - ~ 0.5 mm
Fifth Generation	1993 onward	<ul style="list-style-type: none"> - Textured - Anatomically-shaped - Implant stabilization 	<ul style="list-style-type: none"> - Highly cross-linked, cohesive silicone - Form-stable 	<ul style="list-style-type: none"> - Manufacturer-specific - Low bleed-through rate
Polyurethane	1968 onward	<ul style="list-style-type: none"> - Internal Y-shaped baffle (Natural-Y) - PU foam - Micro-PU foam (Microthane) 	<ul style="list-style-type: none"> - Manufacturer-specific 	<ul style="list-style-type: none"> - ~ 1.5 mm
Double Lumen	1976 onward	<ul style="list-style-type: none"> - Textured/smooth 	<ul style="list-style-type: none"> - Silicone inner, saline outer - (vice-versa for Mentor Becker) 	<ul style="list-style-type: none"> - Unknown
Trilucent	1995–1999	<ul style="list-style-type: none"> - Open-cell textured 	<ul style="list-style-type: none"> - Soybean oil triglycerides 	<ul style="list-style-type: none"> - Unknown
Poly Implant Prothèse	1997–2010	<ul style="list-style-type: none"> - Textured/smooth 	<ul style="list-style-type: none"> - Low-quality industrial-grade silicone gel 	<ul style="list-style-type: none"> - Unknown - Significant variation within sample and between samples
Diagon/Gel 4Two	2010 onward	<ul style="list-style-type: none"> - Textured - Micro-PU foam (Microthane) 	<ul style="list-style-type: none"> - Softer gel on the posterior aspect - Firmer gel on the anterior aspect 	<ul style="list-style-type: none"> - Unknown
Sixth Generation	2010 onward	<ul style="list-style-type: none"> - Smooth (~ 4 μm) 	<ul style="list-style-type: none"> - Manufacturer-specific - Ergonomic and rheological filler (Motiva) 	<ul style="list-style-type: none"> - Manufacturer-specific - ~ 0.5 mm (Motiva) - Advanced multilayered elastomer shell (GC Aesthetics)
B-Lite	2015 onward	<ul style="list-style-type: none"> - Textured/smooth 	<ul style="list-style-type: none"> - Inert hollow borosilicate beads 	<ul style="list-style-type: none"> - Unknown

BI, Breast implant; LMWC, Low molecular weight chain; HMWC, High molecular weight chain; PU, Polyurethane.

250 action.⁹⁷ These BIs include Motiva Silk Smooth, Sebbin Integrity and Sublimity, and Nagor Perle lines.
251 Despite a smooth outer surface according to ISO-14607:2018,⁹⁸ they present peculiar biomimetic to-
252 pography, different from previous smooth implants,^{99,100} which aims at reducing bacterial growth
253 and inflammatory response compared to macrotextured devices, all the while minimizing host re-
254 sponse.^{101,102} Other innovative features of new generation devices include the ergonomic and rheo-
255 logical filler gels which change shape and projection according to the position,¹⁰³ or advanced multi-
256 layered elastomer shells to minimize silicone diffusion.¹⁰⁴

257 Another filler innovation was introduced in 2015 as a lightweight alternative to traditional silicone,
258 implant named B-Lite, manufactured by the Israeli company G&G Biotechnology Ltd. and owned by
259 POLYTECH Health & Aesthetics GmbH since 2018. They are silicone-filled BIs, with smooth or tex-
260 tured surface, that use innovative microsphere technology to disperse inert hollow borosilicate beads
261 throughout its filler silicone, resulting in a lighter implant for a given volume.¹⁰⁵ On February 2021,
262 B-Lite received a temporary CE mark suspension due to the concern for the presence of filler gel with
263 beads, larger than 30µm, on the outer shell of the devices. It is unclear whether was the filler bleed-
264 ing through the implant shell or touching the outer surface during manufacturing. Nevertheless, the
265 suspension was meant to last 3 months, and eventually the CE mark was reinstated,¹⁰⁶ but so far
266 B-Lite are not yet available on the market and still have not received the FDA approval (Table 1).

267 As of today in absence of proper obligatory or opt-out breast implants registries, it can only be
268 approximately estimated that millions of BIs are sold and implanted, assisting plastic surgeons in
269 their pursuit to offer solutions in difficult clinical reconstructive and esthetic cases. Most women are
270 pleased with their implants, and those on the market today are considered safe by regulatory au-
271 thorities. Nevertheless, history teaches us that only vigorous manufacturing processes, investment in
272 innovation, and attentive vigilance can help us maintain these devices safe and available.

273 On the basis of previous failures and innovations, the latest frontier for implant is 3D bioprinting
274 technology, which uses cells and growth factors as the “ink” to create structures that resemble natural
275 tissues such as fat and blood vessels.^{107,108} The promise of these technologies has the ultimate goal
276 of producing de novo organs for transplantation.¹⁰⁹ The near future might also bring us the use of
277 scaffolds that can act as standalone devices, functioning as temporary carriers for autologous tissues,
278 where adipocytes introduced through fat transfers replace the scaffold over time.¹¹⁰ Polycaprolactone
279 has been recently found on a preclinical level as a successful biomaterial for breast tissue engineer-
280 ing.^{111,112}

281 In conclusion, it is only by understanding the past of BIs that we can expect to move forward with
282 innovative designs and refinements which will ultimately benefit patients' health and satisfy their
283 esthetic expectations.

284 Ethical approval

285 Not required.

286 Declaration of Competing Interest

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299 **References**

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