# Vestibular rehabilitation training in patients with subacute stroke: A preliminary randomized controlled tria

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#### 11 Abstract.

- BACKGROUND: Vestibular rehabilitation (VR) consists in a customized exercise program patient-centred that includes a
- combination of different exercise components with the aim to promote gaze stability, improve balance and gait, and facilitate
   somatosensory integration.
- **OBJECTIVE**: The aim of this study was to investigate the effect of customized vestibular rehabilitation training on gait stability of patients with subacute stroke.
- METHODS: Twenty-five inpatients (12 M, age:  $64.1 \pm 12.1$  years) with diagnosis of subacute stroke were enrolled and
- randomized in two groups. All patients were evaluated before and after 4 weeks of training sessions. An instrumented 10-
- <sup>19</sup> Meter Walk Test together with traditional clinical scales were used to assess VR effects. To investigate if any fall event
- <sup>20</sup> occurred after patients' dismissal, they were followed-up at three and twelve months after dismissal.
- RESULTS: Higher values of walking speed and stride length were observed in the VR group. Conversely, no significant
- difference was found in terms of trunk stability. The results of between-group comparison highlight significant differences between the two groups for different clinical scale scores.
- CONCLUSION: VR could be included into a rehabilitation program for patients with stroke for improving their gait and
   dynamic balance acting on their vestibular system as facilitator of recovery.
- 26 Keywords: Vestibular rehabilitation, stroke, instrumented assessment, dynamic balance and gait

# 27 **1. Introduction**

Vestibular rehabilitation (VR) is an exercise program patient-centred that includes a combination
 of different exercise components with the aim to

promote gaze stability, improve balance and gait, and facilitate somatosensory integration (Han et al., 2011). Recent reviews report evidence to support the use of VR in people with unilateral peripheral vestibular disorders (McDonnell et al., 2015) and with bilateral vestibular loss, for supporting balance and gaze stability training (Hall et al., 2016). In addition, some efficacy of VR in reducing risk of fall in patients with vestibular hypofunction and in older adults has been reported (Martins et al., 2016).

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Neurological patients, such as those with Parkinson's disease, multiple sclerosis, and cerebral palsy,
who undergo a VR program, show an improvement in
static and dynamic balance (Acarer et al., 2015), quality of life (Hebert et al., 2011), functional capacity
(Hebert et al., 2011), and motor control (Tramontano
et al., 2017).

Among neurologic diseases, stroke is one of the 48 most common cause of long-term adult disability 49 (Duncan et al., 2003) leading to cognitive and motor 50 function impairments. Particularly, gait and balance 51 disorders may contribute to immobility and falls 52 (Marsden et al., 2005). The design of personalized 53 rehabilitation protocols, especially in the subacute 54 phase of the stroke event, focused on the recovery 55 of dynamic balance ability would be fundamental 56 to reduce these deficits and, consequently, the risk 57 of falling, thus improving patients' quality of life 58 (Iosa et al., 2012; Iosa et al., 2012). In this respect, 59 a recent study indicated that vestibular rehabilitation 60 might improve vestibulo-ocular reflex (VOR) in 61 patients with stroke, highlighting a positive effect 62 of this VOR improvement also on gait performance 63 (Mitsutake et al., 2017). This result was also sup-64 ported by neurophysiological findings: the vestibular 65 cortical network, in fact, contributes to modulate 66 space, body, and self-awareness, spatial navigation, 67 and reflex generation for posture and oculomotor 68 control (Lopez et al., 2016). This network is in close 69 convergence with other sensory and motor signals, 70 attention, memory, mental imagery, and even social 71 cognition (Angelaki et al., 2008; Angelaki et al., 72 2009). In addition, subliminal galvanic vestibular 73 stimulation induces long-term reduction of hemi-74 spatial neglect and improves vertical perception in 75 stroke patients (Oppenländer et al., 2015). Despite 76 this evidence, no studies have considered the use of 77 VR programs to improve dynamic balance in gait in 78 patients with stroke. 79

Under these premises, the aim of this study was to investigate the effect of customized vestibular rehabilitation training on gait stability of patients with subacute stroke. We hypothesized that a neurorehabilitation training including vestibular rehabilitation might improve gait and dynamic balance also in patients with subacute stroke.

## 87 2. Methods

## 88 2.1. Participants

Twenty-five inpatients (12 M, age:  $64.1 \pm 12.1$ years) with diagnosis of subacute stroke were enrolled in this study and randomized in two groups (Fig. 1). This sample size complied with the minimum number of participants recommended by a power analysis purposely performed ( $\alpha = 0.05$ ;  $\beta = 0.8$ ; ES = 0.5) for non-parametric between-groups comparisons (Cohen, 1977). According to this sample size estimation procedure, the inclusion of at least 8 patients for each group is recommended. Therefore, a Vestibular Group (VG) was composed of 13 inpatients (8 M, age:  $63.1 \pm 8.5$  years) and a Control Group (CG) was composed of 12 inpatients (4 M, age:  $65.1 \pm 15.5$  years, p = 0.700, *t*-test). Demographic characteristics of the sample are reported in Table 1.

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Inclusion criteria were: stroke with unilateral hemiplegia occurred within the previous six months and ability to walk without any device or need of continuous physical assistance to support body weight or maintain balance (Functional Ambulation Classification >3). Exclusion criteria were: cognitive deficits affecting the capacity of patients to understand the task instructions (Mini Mental State Examination >24); severe unilateral spatial neglect (diagnosed with a battery of test including Letter Cancellation test, the Barrage test, the Sentence Reading test and the Wundt-Jastrow Area Illusion Test), severe aphasia (diagnosed with neuropsychological assessment), and presence of neurological, orthopedic or cardiac comorbidities (all of them clinically evaluated).

This study was approved by the Local Independent Ethics Committee and all participants gave their written informed consent to participate in the study.

#### 2.2. Experimental protocol

The study was conducted at the Neurorehabilita-126 tion Hospital "Fondazione Santa Lucia" from March 127 2015 to January 2017. All patients were evaluated 128 before the training (T0) and at the end of the training 129 (T1) sessions. To investigate if any fall event occurred 130 after patients' dismissal, they were followed-up by 131 phone interviews, made by the same physiothera-132 pist, at three and twelve months after their dismissal 133 (Morone et al., 2014). Patients were asked if they 134 experienced any fall and, eventually, to describe how 135 and why it happened. Both VG and CG performed 136 a standard physiotherapy program (2 times/week for 137 4 weeks). In addition, 12 rehabilitation sessions (3 138 times/week for 4 weeks) of 20 minutes were admin-139 istered to both groups: VG performed vestibular 140

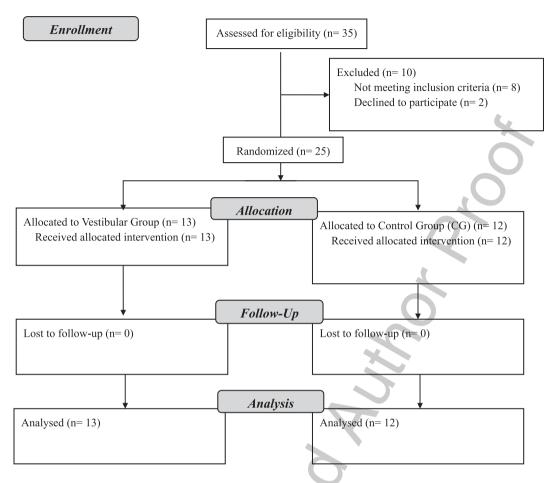


Fig. 1. Flow Diagram.

Table 1 Demographic and clinical characteristics at baseline

	VR	CG
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Age Gender	$63.1 \pm 8.5$	$65.1 \pm 15.5$
	8M; 5 F 65.6 ± 13.3	4M; 8F $68.4 \pm 13$
Mass (kg) Stature (cm)	$05.0 \pm 15.5$ $171.3 \pm 9.1$	$68.4 \pm 13$ 165.7 ± 7.5
Stature (Cm) Stroke location		7  right; 5 left
Stroke location	6 right; 7 left	7 fight; 5 left

VR: Vestibular Rehabilitation Group, CG: Control Group.

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rehabilitation with exercises aiming at enhancing gaze stability and upright postural control (Han et al., 2011) (cfr. Interventions section). For CG additional rehabilitation training was focused on trunk stabilization and weight transfer to the paretic leg.

An expert physician, blind to patients' allocation, assessed each patient using the following clinical scales: Functional Ambulation Classification (FAC) (Holden et al., 1984), Tinetti Balance and Gait (TBG) (Tinetti et al., 1986), Berg Balance Scale (BBS) (Berg 1992), and Barthel Index (BI) (Collin et al., 1988).

All patients provided written informed consent and 153 accepted to perform an instrumented 10-Meter Walk 154 Test (10-MWT), for three times consecutively, on a 155 straight pathway at their self-selected walking speed, 156 at both T0 and T1. The experimental protocol of this 157 instrumented assessment was selected according to 158 a previous study (Bergamini et al., 2017) using five 159 Inertial Measurement Units (IMUs) (Opal, APDM 160 Inc., Portland, Oregon, USA) and 3D linear accelera-161 tions and angular velocities were collected. Each unit 162 embedded three-axial accelerometers and gyroscopes 163  $(\pm 6 \text{ g with } g = 9.81 \text{ m} \times \text{s}^{-2}, \text{ and } \pm 1500 \text{ °/s of full-}$ 164 range scale, respectively) and provided the measured 165 quantities with respect to a unit-embedded system of 166 reference. To assess gait stability, three IMUs were 167 secured to the participants' upper body: one on the 168 occipital cranium bone of the head (H), one on the 169 center of the sternum body (S), and one at L4-L5 level, 170 slightly above the pelvis (P) (Fig. 2). The other two 171 units were located on both distal tibiae (lateral malle-172 oli) and were used to perform stride segmentation. 173

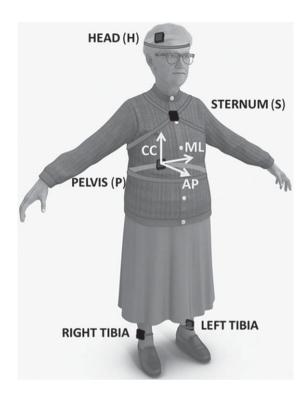


Fig. 2. Location of the Inertial Measurement Units (IMUs) attached on the participants' body segments. The axes orientation of the pelvis (P), sternum (S), and head (H) IMUs was the same during the static phase at the beginning of each trial. For the sake of clarity only the orientation of the pelvis unit is depicted (AP, antero-posterior; ML, medio-lateral; CC, cranio-caudal). Adapted from "Multi-sensor assessment of dynamic balance during gait in patients with subacute stroke" by Bergamini E et al. J. Biomech. (2017), http://dx.doi.org/10.1016/j.jbiomech.2017.07.034.

To limit the relative movement between the units and 174 the underlying skin, IMUs were secured to the rele-175 vant body segment using ad hoc supports (a swim cap 176 with a tailored pocket for the head IMU and elastic 177 straps for the other units). To guarantee a repeat-178 able reference system for the three IMUs located 179 on the upper body, each unit was aligned with the 180 corresponding anatomical axes (antero-posterior: AP, 181 medio-lateral: ML, and cranio-caudal: CC) following 182 the procedure proposed by (Bergamini et al., 2017). 183

For each 10-MWT, the following spatiotemporal 184 parameters were obtained: average walking speed 185 (WS = 10 m/time to complete the test), average stride 186 length (SL = 10 m/total number of strides), and stride 187 frequency (SF = total number of strides/time to com-188 plete the test). For what concerns gait stability, only 189 steady-state strides were analyzed, and the following 190 parameters were estimated: 191

• Attenuation Coefficients (Mazzá et al., 2008) (AC) between each level pair (H, S, P), for each acceleration component (AP, ML, CC). Each coefficient represents the variation of the acceleration from lower to upper levels of the upper body. A positive coefficient indicates an attenuation of the accelerations from the lower to the upper level, whereas a negative coefficient indicates an amplification.

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- Improved Harmonic Ratio (Pasciuto et al., 2017) (iHR) for each acceleration component (AP, ML, CC) measured at the pelvis level. This index is a measure of gait symmetry and is based on a spectral analysis of the acceleration signals (0%, total asymmetry; 100%, total symmetry).
- 2.3. Interventions

# 2.3.1. Balance exercises (CG only)

The balance exercises were focused on trunk stabilization and weight transfer to the paretic leg and consisted of three exercises. First, patients were seated blindfolded on a Bobath ball for 5 minutes with an expert physiotherapist supporting them in keeping the right position. Second, patients were asked to maintain balance in a standing position on a Freeman board for 5 minutes. The third exercise consisted in transferring body weight to the paretic leg using parallel bars for 10 minutes (Morone et al., 2014).

# 2.3.2. Gaze stability exercises (VG only)

Exercises were performed staring at a static object while participants turned their head side to side and up and down (VORx1) (Herdman et al., 1989) for one minute for each axis. The exercises were carried out for no more than 10 min including quick rest period and were performed seated, standing and during a step on the spot. One physiotherapist, specifically trained in VR, checked that patients maintained gaze stability during each task.

#### 2.3.3. Upright postural control (VG only)

Each patient was asked to get on a 5 cm thick foam cushion and then was blindfolded. Once the patient was in a stable posture, he/she was given the following instruction: "step on the spot for one minute". At the end of the first minute, remaining blindfolded, the patient made  $90^{\circ}$  clockwise turn and repeated the exercise for another minute. The same procedure was carried out at  $180^{\circ}$  and  $270^{\circ}$  for a total of four minutes. In case patients rotated (left/right) or moved
(forward/backward) during the stepping execution,
the physiotherapist helped them to recover the original position using verbal cues (e.g., "you are turning
left/right" and "you are moving forward/backward")
(Tramontano et al., 2016). The maximum exercises
duration was of 10 min, including quick rest periods.

#### 245 2.4. Statistical analyses

The IBM SPSS Statistics software (v23, IBM 246 Corp., Armonk, NY, U.S.A.) was used. A normal-247 ity check was performed using the Shapiro-Wilk test. 248 Due to lack of normality for all the above-mentioned 249 parameters, median and inter-quartile ranges were 250 used to summarize all the computed parameters and 251 all data were then analyzed using non-parametric 252 statistics. In particular, Mann-Whitney U-test was 253 used to compare data between groups and Wilcoxon 254 Signed Ranks test was used for within-group analy-255 ses. The alpha level of statistical significance was set 256 at 0.05 for all the tests. 257

### 3. Results

Table 2 shows the scores of the clinical scales administered before (T0) and after (T1) the rehabilitation program. At T0, no statistically significant differences were observed between the two groups. The results of between-group comparison at T1 highlighted that all clinical scale scores were higher in VG than in CG. Specifically, significant differences were found for the Tinetti total score and Tinetti gait subscore (p=0.011 and p=0.014, respectively). In addition, the results of the Wilcoxon Signed Ranks test showed that the scores of all scales increased for both groups (p<0.05), for the sake of clarity, the within-group analysis results are not displayed in Table 2.

In Table 3, the results of the instrumented gait analysis are reported. For what concerns the between groups analysis, VG and CG resulted homogenous at T0 also in terms of walking ability. At T1, significant differences were found for both WS (p = 0.043) and SL (p = 0.009), which resulted higher in VG than

Table 2

Median and interquartile range (IQR) of clinical scale scores pre- and post-rehabilitation (MBI: Modified Barthel Index, FAC: Functional Ambulation Classification, T-Total: Tinetti scale, T-Balance: Tinetti Balance subscale, T-Gait: Tinetti gait subscale, BBS: Berg Balance Scale, RMI: Rivermead Motricity Index). *P*-values report the results of Mann-Whitney u-test (in bold and with asterisk if statistically significant)

Scale	Pre – Rehabilitation (T0)			Post – Rehabilitation (T1)			
	VG	CG	<i>p</i> -value	VG	CG	<i>p</i> -value	
MBI	$89.1 \pm 11.1$	$85.8 \pm 12.7$	0.503	97.8±4.7	$95.8\pm5.2$	0.137	
FAC	$3.6 \pm 0.5$	$3.5 \pm 0.5$	0.650	$4.4 \pm 0.5$	$4.1 \pm 0.5$	0.270	
T-total	$21.9\pm3.9$	$20.2 \pm 3.1$	0.137	$26.5\pm1.5$	$23.8\pm2.8$	0.011*	
T-Balance	$12.7\pm2.6$	$11.8\pm2.2$	0.295	$15.2 \pm 1.4$	$13.8\pm1.7$	0.060	
T-Gait	$9.2 \pm 1.5$	$8.3 \pm 1.4$	0.137	$11.4\pm1.0$	$9.9 \pm 1.4$	0.014*	
BBS	$44.8\pm6.4$	$40.9 \pm 6.1$	0.137	$51.5 \pm 3.3$	$48.0 \pm 4.7$	0.060	
RMI	$9.7\pm2.0$	$9.3 \pm 2.4$	0.769	$13.2\pm1.2$	$12.5\pm1.5$	0.186	

#### Table 3

Median and interquartile range (IQR) values of instrumented gait parameters pre- and post-rehabilitation (WS: walking speed, SF: stride frequency, SL: stride length, AC<sub>PH</sub>: coefficient of attenuation of acceleration between pelvis and head, iHR: improved harmonic ratio, AP: antero-posterior axis, ML: medio-lateral axis, CC: cranio-caudal axis). *P*-values report the results of Mann-Whitney U-test (in bold and with asterisk if statistically significant)

Gait Parameter	Pre – Rehabilitation (T0)			Post – Rehabilitation (T1)		
	VG	CG	<i>p</i> -value	VG	CG	<i>p</i> -value
WS	$0.71 \pm 0.14$	$0.57 \pm 0.15$	0.083	$0.78\pm0.14$	$0.61\pm0.14$	0.043*
SF	$0.67\pm0.07$	$0.66 \pm 0.06$	0.999	$0.68\pm0.08$	$0.68\pm0.10$	0.700
SL	$1.06 \pm 0.17$	$0.87 \pm 0.20$	0.100	$1.15\pm0.17$	$0.90\pm0.15$	0.009*
ACPH-AP	$25.1\pm40.4$	$11.8\pm28.5$	0.178	$31.8\pm29.1$	$8.97 \pm 41.8$	0.211
ACPH-ML	$-3.6 \pm 48.8$	$17.1 \pm 12-1$	0.501	$10.5\pm37.2$	$-1.6\pm44.9$	0.386
AC <sub>PH</sub> -CC	$2.6\pm9.7$	$2.2\pm16.0$	0.847	$2.8\pm10.5$	$3.2 \pm 10.0$	0.923
iHR-AP	$85.6\pm10.3$	$77.0 \pm 11.6$	0.083	$89.5\pm5.8$	$72.5\pm30.0$	0.923
iHR-ML	$69.9 \pm 9.5$	$68.4 \pm 5.5$	0.501	$67.5 \pm 13.9$	$62.5\pm26.0$	0.124
iHR-CC	$85.5\pm5.4$	$75.0\pm13.6$	0.102	$87.3\pm7.1$	$73.5\pm30.4$	0.211

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in CG. When considering the within-group analysis, no significant differences were found, even if
an increasing trend was observed in VG for all
gait parameters. Conversely, CG displayed only a
decreasing trend of the AP and ML components of
AC as well as of all three components of iHR.

Three patients of CG fell at least two times twelve months after their dismissals and one patient of VG fell one time twelve months after his dismissals.

# 288 **4. Discussion**

This study tested the use of a vestibular rehabilita-289 tion protocol aimed at enhancing gait and dynamic 290 balance in patients with subacute stroke. Results 291 show a significant improvement in Tinetti Balance 292 Gait scores in patients who underwent a customized 293 vestibular rehabilitation program. These results are in 294 accordance with those of Mitsutake and co-workers 295 showing that 3 weeks of vestibular rehabilitation 296 in subacute stroke subjects have positive effects on 297 patients' balance ability during walking (Mitsutake et 298 al., 2017). Instrumented analysis of walking showed 299 higher values of walking speed and stride length in the 300 VR group. Conversely, no significant difference was 301 found in terms of trunk stability. This result could be 302 due to the actual reduced sample size, because only 303 a subgroup of patients accepted to be tested using 304 instrumented gait analysis. Interestingly, despite the 305 higher speed at which the VR group walked at T1, 306 they were able to maintain similar upper body stabil-307 ity and symmetry with respect to the slower control 308 group. The above-mentioned trend observed in the 309 VR group goes towards increased AC and iHR that 310 are typical of mild severity in stroke (Bergamini et 311 al., 2017; Belluscio et al., 2017). 312

Hence, VR showed some slight higher effect than 313 conventional therapy. A possible role played by the 314 reflex mechanism related to vestibular function in 315 postural control and gait performance could be at 316 the basis of these results, as confirmed by previous 317 studies showing the relationship between gaze sta-318 bilization function and gait performances (Whitney 319 et al., 2009; Hillman et al., 1999) in patients with 320 vestibular deficit. Moreover, the vestibular-spinal 321 tract is thought to play a significant role during the 322 execution of voluntary forward steps (Bent et al., 323 2002) in a specific stance phase (Bent et al., 2005). 324 Vestibular information is weighted more heavily dur-325 ing double support than at any other time of the gait 326 cycle (Bent et al., 2005) giving more stability during 327

all gait cycle. In other words, the vestibular system can primarily induce a modulation of antigravitary muscles and balance reactions (Nallegowda et al., 2004) that, in turn, can be learned and used by feedforward mechanisms prior to voluntary movements during gait. Patients with stroke often experience balance disorders (Iosa et al., 2012), furthermore they may also have difficulties in an adequate utilization of vestibular information and their balance and gait function is mainly based on visual input (Bonan et al., 2004). VR, modulating neuroplasticity in the vestibular network, might have promoted a sensory reweighting in our patients improving their walking performance. Even in absence of a specific vestibular damage, as in the sample enrolled in the present study. VR seems to act as a facilitator for improving a compensation strategy based on the enhancement of vestibular functions for managing a correct trade-off between stability and advancement during gait (Iosa et al., 2016).

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Despite the increased interest in evaluating and investigating the effects of vestibular network on balance and waking dysfunction (Van Wyk et al., 2016), so far, only one study analysed the effects of VR in stroke (Mitsutake et al., 2017). Our study suggests that the integration of vestibular rehabilitation in a standard post stroke rehabilitation protocol has the possibility to boost dynamic balance and walking recovery. Another key to interpretation of our results is that the mechanisms of experience-dependent plasticity contribute to post-stroke neuronal reorganization and to the efficacy of rehabilitative training, so it could be speculated that a need of stimulating the vestibular system exists for obtaining an increase in stability or, as our results suggest, the capacity of patients to walk faster without decreasing their upper body stability (Allred et al., 2014).

The idea of stimulating an undamaged apparatus to favour the recovery of a multi-systemic ability such as walking is not entirely new. A recent RCT (Van Wyk et al., 2014) investigated the effects of visual scanning exercises with saccadic eye movement training during task-specific activities for patients with Neglect following a stroke. As suggested by the authors, although the intervention was focused on the visual system (visual scanning exercises integrated with task-specific activities), they found more general positive effects, probably due to the inner integration of visual system with the vestibular and the somatosensory (proprioceptive, cutaneous, and joint receptors) systems in maintaining postural orientation and stability during functional movement. An encouraging result was the lower trend in number of falls observed in the VG group twelve months after dismissals. Presumably, this result reveals that a dynamic balance training could improve the balance confidence and the self-perception reducing the risk of falls (Morone et al., 2014).

Our study has some important limitations. 386 Although the sample size was defined according to 387 the results of a power analysis, it was shown to be 388 rather small. It can be speculated that the number of 389 significant differences would increase if the sample 390 size would be enlarged. This is particularly evident 391 for what concerns the instrumented analysis results, 392 where not all patients signed the informed consent 393 for that test. Another limitation is the absence of a 394 neurophysiological measure of potential vestibular 395 deficits. This measure was not considered because 396 it has been hypothesized that VR had an effect on 397 dynamic balance regardless a specific damage of the 398 vestibular system. However, as this measure could 399 be helpful for obtaining a clearer patients' clini-400 cal picture, further studies should take this aspect 401 into account. Another limitation concerns vestibular 402 training, because we used only active horizontal and 403 vertical head movements. Indeed, previous studies 404 indicate that compensatory strategies should incorpo-405 rate passive rotations (Cullen et al., 2004; Schubert et 406 al., 2008) and it could be interesting for further studies 407 to investigate also the effects of a new rehabilitation 408 paradigm with passive rotations training. 409

In conclusion, VR could be included into a rehabilitation program for patients with stroke for improving
their gait and dynamic balance acting on their
vestibular system as facilitator of recovery, hopefully
reducing their risk of falling.

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# 420 **Conflict of interest**

The authors declare no competing financial interests.

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## **Ethics approval**

The study was approved by Local Ethics Committee of IRCSS Fondazione Santa Lucia.

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