

1 Structural and thermal characterization of zirconia/hydroxyapatite composites
2 prepared via sol-gel for biomedical applications
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25 **Abstract**

26 The thermal behavior of pure ZrO₂ and hydroxyapatite (denoted as Z and HAp, respectively), as
27 well as three composites with different content of Z and HAp (Z90HAp10, Z70HAp30 and
28 Z50HAp50) prepared via sol-gel method has been studied by thermogravimetry (TG) and first-order
29 derivative of TG up to 1200°C under inert gas atmosphere. Dehydration, loss of alcohol and
30 acetylacetone and a multi-step thermal decomposition processes has been identified by analyzing
31 the gases evolved in each step by Fourier transform infrared spectroscopy (FTIR). Fresh samples of
32 Z-rich composites undergo an abrupt ejection of material from the crucible around 200°C with
33 noticeable increase of the sample temperature. During the occurrence of this phenomenon FTIR
34 spectra demonstrated the evolution of gases (CO, CO₂, acetone and ethylene) due to the
35 simultaneous decomposition of acetylacetone and ethanol, not present in the samples calcined at
36 120°C. As far as the structural study is concerned, pure Z crystallizes at 1000°C in the monoclinic
37 system, but the presence of HAp in the composite materials enables the crystallization of Z in the

38 tetragonal phase. Finally, the amorphization degree increases with increasing the content of Z in all
39 the composites treated at 600 and 1000°C.

40

41 **Keywords:** sol-gel process; hydroxyapatite; crystallization of zirconia; TG-FTIR analysis

42 **1. Introduction**

43 Glass and ceramics with several compositions are materials widely proposed for biomedical
44 applications, mainly in dental and orthopedic fields. Bioactive glasses, indeed, exhibit ability of
45 forming biominerals on their surface, which attracts bone building osteoblast cells. From the
46 development of the first bioglass by Hench at al. (denoted as 45S5), many compositions of
47 bioglasses were explored in order to obtain biomaterials with enhanced performance. Among these,
48 zirconia (ZrO_2) and zirconia-based glasses and ceramics, as well as calcium phosphates, with
49 particular reference to hydroxyapatite (HAp), have attracted considerable interest in the recent years
50 [1-10]. Their use, indeed, have several advantages. Studies proved that when zirconia-based
51 prosthesis were implanted in vivo, they are encapsulated by connective tissue and, thus, no local or
52 systemic toxic effects were recorded neither in soft nor in hard tissues after their implantation [3, 5].
53 Moreover, no release of residues or degradation phenomena were detected and a low bacterial
54 growth was recorded [3, 5].

55 Both crystalline and amorphous zirconia and zirconia-based materials have shown interesting
56 biological performances. Amorphous zirconia-based glasses were proposed as matrices for drug
57 delivery [2, 11], or as bioactive coatings [12-15], showing the ability to improve cell viability of
58 human osteosarcoma cell line [13] and human mesenchymal stromal cells [15]. Yttrium-stabilized
59 tetragonal zirconia or tetragonal zirconia polycrystal (TZP) was used in orthopaedics (as hip head
60 prostheses) [16], and in dentistry for root canal posts, fixed partial dentures and dental implants
61 [17]. On the other hand, as far as the biomedical applications are concerned the interest in calcium
62 phosphate-based ceramics [4, 18-23] for bone repair and substitution stems from their bioactivity
63 (i.e. the capability to bond with the living bone by the formation of an hydroxyapatite layer on their
64 surface with a composition similar to that of the mineral phase of bone [24]). In particular, the
65 interest for crystalline HAp and HAp-based ceramics as materials for artificial bones and scaffolds
66 for tissue engineering [25], is due to their similarity with biological apatites present in bones and
67 teeth that leads to high affinity with host tissue and, thus, to an excellent bioactivity and

68 biocompatibility. However, their poor mechanical properties that limit their usage in several clinical
69 application, induced researchers to develop composites consisting of synthetic hydroxyapatite and
70 TZP fillers to reinforce the HAp structure [26-29]. Moreover, composites mainly consisting of
71 zirconia containing different amount of synthetic HAp were recently proposed [30], where addition
72 of HAp led to an improvement of the biological performance of pure zirconia. The ZrO_2 /HAp
73 composites were obtained by mean of the sol-gel method, a process used to manufacture glass and
74 ceramic oxides at low temperature. The synthesis procedure involves the hydrolysis of a metal
75 alkoxide precursor dissolved in a water-alcohol solution and the condensation of the formed
76 oligomers. Those reactions cause the transition from the starting colloidal solution named “sol” into
77 a 3D network, namely “gel”. A heat treatment of the gel is required to allow the removal of the
78 residual solvents and the densification of the materials. Modifying the gel heating conditions results
79 in modulating the structure and, thus, the properties of the obtained materials. The temperature and
80 heating rate of the heating treatment, indeed, are well known key factors in determining the final
81 microstructure of glass and ceramic sol-gel materials. For example, a xerogel can be obtained using
82 low temperatures, whereas solvent extraction under supercritical conditions is requested to produce
83 an aerogels. Moreover, different heating conditions can lead to amorphous or crystalline materials.
84 As a different degree of crystallization leads to a variation of the ion release from the materials, it
85 can influence also material biological performances as observed for ZrO_2 /HAp composites and
86 other sol-gel bioglasses [30, 31]. The dissolution rate of a bioactive glass, indeed, plays a key role
87 in its usage as implant because can cause alterations in the mechanical properties of the material as
88 well as variation in its surface charge, thus leading to a modification in the protein adsorption and
89 hydroxyapatite nucleation ability.

90 Therefore, the in-depth knowledge of thermal decomposition of the dried gels is essential and the
91 determination of the optimum condition for the calcination of the sol-gel materials is required to
92 obtain the desired biomaterial [32-38]. The present study inserts in this context and has the aim of
93 investigating into the thermal degradation phenomena and the structural modifications that take

94 place when the previously synthesized sol-gel ZrO₂/HAp composites [30] were submitted to
95 heating. To this end, the thermal behavior and the mechanisms of the thermally stimulated
96 processes were studied by evolution gas analysis (EGA), similarly to what has been carried out in
97 the past [39]. In this study, the EGA system has been realized by coupling a thermal analysis
98 equipment with a Fourier transform infrared spectroscopy (FTIR) unit. This information is
99 necessary to explain the relation between the different biological responses recorded after exposure
100 to the materials and the temperatures of the applied post-synthesis heat treatments, and to identify
101 the better conditions to be used for obtaining bioimplants with relevant biological performances.

102

103 **2. Materials and methods**

104 *Sol-gel synthesis*

105 Composites with chemical formula xZrO₂(1-x)HAp (where x = 1, 0.9, 0.7, 0.5, 0 indicates the mole
106 fraction of ZrO₂ in the composites) were synthesized by means of the sol-gel method as reported
107 elsewhere [30]. The pure ZrO₂ was obtained using a zirconium propoxide solution (70 wt. % in 1-
108 propanol, Sigma-Aldrich, Milan, Italy) as metal alkoxide precursor. The precursor was added to a
109 solution of acetylacetone (AcAc, Sigma-Aldrich, Milan, Italy), a chelating agent used to inhibit the
110 fast hydrolytic activity of zirconium propoxide, in pure ethanol (99.8% Sigma-Aldrich, Milan,
111 Italy). The molar ratios between the reagents achieved in the obtained sol are the follows:
112 $Zr(OCH_2CH_2CH_3)_4 / AcAc = 3$ and $EtOH / Zr(OCH_2CH_2CH_3)_4 = 6$.

113 To synthesize pure HAp, calcium nitrate tetrahydrate (Ca(NO₃)₂ · 4H₂O, Sigma-Aldrich, Milan,
114 Italy) and phosphorus pentoxide (P₂O₅, Sigma-Aldrich, Milan, Italy) were used as precursor, where
115 Ca(NO₃)₂ · 4H₂O was dissolved in pure ethanol under magnetic stirring. The resulting solution was
116 then added under stirring to a previously prepared solution of P₂O₅ in NH₄OH and pure ethanol at
117 pH=11, thus obtaining a molar ratio Ca/P in the final solution equal to 1.67.

118 The composites samples were synthesized by adding drop by drop and under stirring adequate
119 amounts of zirconia sol to the HAp one, until a homogeneous and transparent solution was

120 obtained. Then, the composites sols were left to gel at room temperature and the obtained wet gels
121 dried at 40°C for 2 hours.

122

123 *Thermal and evolution gas analyses*

124 The thermal behavior of the pure ZrO₂, HAp and composites was studied by means of a
125 simultaneous Mettler Toledo TG/DSC 2950 instrument, being the experimental raw data processed
126 by a STARe software. The instrument has been equipped with two identical crucibles, one for the
127 reference filled with alumina in powder form and one for the sample, containing about 20–25 mg of
128 solid in order to uniformly cover the bottom surface area of the crucible. The TG experiments were
129 carried out under an inert nitrogen flowing atmosphere (60 mL min⁻¹) up to 1200 °C at a heating
130 rate of 10°C min⁻¹. The sample temperature was calibrated by performing identical experiments
131 using very pure indium and zinc reference materials (purity higher than 99.998%), and assuming a
132 final average uncertainty $u(T)=\pm 1\text{K}$ over the whole temperature range explored.

133 The mechanisms of thermally activated processes during the occurrence of TG/DSC experiments
134 were identified using a SETARAM 92-16.18 TG apparatus coupled by a Thermofisher Scientific
135 Nicolet iS10 Spectrophotometer. The apparatus has been equipped with 250 µL alumina crucibles,
136 filled with about 100-150 mg of sample to obtain the minimum amount of gaseous species to be
137 analyzed by FTIR using the Calisto software. A preliminary blank experiment was performed using
138 empty crucibles under the same experimental conditions of the samples tested (argon purging gas at
139 40 mL min⁻¹, in the temperature range between 25 and 1200°C at a constant heating rate of 10°C
140 min⁻¹). The vapors evolved during the TG experiments were conveyed to the FTIR apparatus
141 through a heated transfer line kept at 200°C. The instrument is able to collect a spectrum each 11 s,
142 being eight scans performed at 0.5 cm⁻¹ intervals with a resolution of 4 cm⁻¹.

143

144 *XRD analysis*

145 After the thermal treatment of the samples powders for 2 h under a argon purge gas atmosphere
146 at 120, 600 and 1000°C (temperatures selected on the basis of a careful examination of their thermal
147 behavior shown by the TG curves), the crystalline phases have been identified by X-ray diffraction
148 (XRD) analysis by means of a Philips diffractometer, equipped with a PW 1830 generator, where
149 the source of X-ray is given by a Cu-K α radiation with $\lambda=0.15418$ nm.

150

151

152 **Results and Discussion**

153 *Thermal behavior study*

154 The TG/DTG curves of fresh samples (not thermally treated) of pure zirconia and HAp (Z and
155 HAp, respectively) and of composites containing different amount of both components (Z90HAp10,
156 Z70HAp30, Z50HAp50) are shown in Fig. 1. In particular, the thermal behavior of pure Z and HAp
157 and Z50HAp50 in Fig. 1a seems to be, as expected. The TG/DTG curves of pure Z, recently
158 examined elsewhere [36], show a first mass loss up to about 150°C, probably due to dehydration.
159 By analyzing the gases evolved during the TG experiment a more complex degradation occurs.
160 The second step of mass loss between 150 and 230°C is mainly due to dehydroxylation that leads to
161 the release of water by condensation of the surface hydroxyl groups. Fig. 1a shows a third step of
162 mass loss between 300 and 470°C, followed by a final step (with about 5% of mass loss) in the
163 range 480-600°C.

164 Pure HAp undergoes a first two-stage process up to about 200°C, accompanied by a mass loss of
165 more than 30%, ascribed to the release of water differently bound to the material. After this
166 process, some slow parallel and consecutive mass losses took place up to 580°C, the first of which
167 seems to proceed through a two-stage pathway between 200 and 380°C, followed by two more
168 distinguishable steps in the temperature ranges 380-490°C and 490-580°C, respectively. The
169 composite material containing equimolar amount of Z and HAp (Z50HAp50) shows a thermal

170 behavior representing a sort of average of those of the pure components, but with more defined and
171 evident effects (DTG peaks are sharper than those of Z and HAp). The total amount of water
172 adsorbed up to 200°C (with three distinct DTG peaks) does not exceed 20%, while the
173 dehydroxylation and degradation steps seem to occur at temperatures higher than those of pure HAp
174 and end at 600°C. On the other hand, the two poor-HAp composites (with 0.1 and 0.3 molar
175 fractions of HAp, denoted as Z90HAp10 and Z70HAp30, respectively) undergo an explosive
176 thermal behavior around 200°C that caused the ejection of significant amount of both the samples
177 from the crucible during their TG experiments, as it can be seen in Fig. 1b. This phenomenon
178 occurred in Z90HAp10 and Z70HAp30 is accompanied by evolution of heat that caused an
179 anomalous increase of the sample temperature with time in comparison with the expected
180 programmed linear one (Figs. 2a-f, particularly evident in Figs. 2c and 2f the black circles).

181 The TG/DTG curves of all the samples (after a thermal treatment at 120°C) are shown in Fig. 3,
182 where a careful examination of their shapes seems to suggest that the thermal treatment at relatively
183 low temperature does not modify significantly the thermal behavior of these composites, except for
184 the absence of the abrupt mass loss occurring in the Z90HAp10 and Z70HAp30, accompanied by
185 evolution of heat and ejection of mass from the crucible. In general, the thermal treatment at 120°C
186 seems to stabilize the two composites (in spite of the relatively low temperature), and the water
187 evolved is partly adsorbed (from water vapor on cooling), and subsequently lost in these TG new
188 experiments at lower temperature (even though because it is probably physically bound to the
189 materials).

190

191 *FTIR-EGA analysis to identify the mechanisms of thermally stimulated processes*

192 Fig. 4 shows the FTIR spectra of the gas mixture evolved during the TG experiments of Z, HAp,
193 and of their composites at different temperatures. In particular, the FTIR spectrum of the gases
194 released from sample Z at 115°C (corresponding to the first step of mass loss in Fig. 1a) revealed an
195 initial evolution of propanol, water and acetone. Propanol is produced by hydrolysis and

196 condensation reactions, which involve zirconium propoxide as precursor, and its release is proved
197 by the intense bands at 2970 cm^{-1} and the doublet at 1065 cm^{-1} , with a shoulder at 980 cm^{-1}
198 ascribable to the stretching of C-H and C-C bonds, respectively, along with the signals in the region
199 $1200\text{-}1500\text{ cm}^{-1}$ ascribable to the C-H bending modes. The stretching of the hydroxyl functional
200 group, generally visible at 3670 cm^{-1} , is covered by the signals of water. At this temperature,
201 indeed, the adsorbed water is also released as proved by the several sharp bands in the ranges 4000-
202 3400 cm^{-1} and $1850\text{-}1280\text{ cm}^{-1}$. In the latter range a strong signal at 1745 cm^{-1} (due to the stretching
203 of C=O bond) is also visible that, together with the peaks at 1220 cm^{-1} and 1365 cm^{-1} (due to C-H
204 and C-C deformations, respectively), proved the formation of acetone. That is the main product of
205 the thermal degradation of the acetylacetone bonded to zirconium (acetylacetonate of zirconium)
206 together with carbon dioxide [40]. Typical signals of CO_2 , indeed, also are visible as a doublet at
207 2355 cm^{-1} , 2320 cm^{-1} and a sharp peak at 670 cm^{-1} . The water signals are still visible in the FTIR
208 spectrum of the gas evolved at 187°C . Moreover, propanol residue is found, whereas the increase of
209 the intensities of the acetone and CO_2 signals suggests that the thermal degradation of acetylacetone
210 continues even at higher temperature. The FTIR spectrum of Z at 378°C reveals in Fig. 4 the
211 intensities of characteristic bands of acetone decreasing, until these signals almost disappear in the
212 spectrum at 523°C . However, at the same time the intensity of bands related to CO_2 increases and
213 the appearance of sharp peaks at 1300 and 3015 cm^{-1} in the spectrum at 523°C suggests that the
214 acetone formed, in turn, degrades leading to the release of methane and CO_2 [40, 41]. Both the
215 mechanisms of the thermal events occurring around 378°C and 523°C are easily identified. The
216 former is related to the initial formation of nucleus of tetragonal zirconia ($t\text{-ZrO}_2$) after
217 dehydroxylation that via condensation of the -OH residue groups located on the materials surface,
218 while the second to the bulk crystallization, in agreement with the literature findings [42]. This
219 hypothesis is also confirmed by the presence of water signals in the FTIR spectra of the gas evolved
220 recorded at 523°C .

221 The FTIR spectrum of the gas evolved during the TG experiment of pure HAp sample at 122°C
222 reveals the presence of water, CO and CO₂. Water released can be due to the removal of the
223 adsorbed, hydration water [43, 44], or by crystallization water contained in calcium nitrate [45], as
224 well as by water produced by the partial combustion of the ethanol [26]. The presence of the signal
225 typical of CO and CO₂ (the doublets at 2355 - 2320 cm⁻¹ and 2230 - 2200 cm⁻¹ respectively),
226 indeed, suggests that an incomplete combustion of organic matter occurs in this material, which
227 could be caused by oxygen released from the materials pore. The spectrum of HAp at 171°C shows,
228 in addition to water, CO and CO₂, the presence of some signals ascribable to other gas species.
229 They appear very noisy because overlapped with the water signals. In particular, the weak bands in
230 the range 3000-2800 cm⁻¹ and those at 1040 cm⁻¹ and 1170 cm⁻¹, indicate that an initial release of
231 ethanol occurs around this temperature. Moreover, the presence of the doublet at 1589 – 1623 cm⁻¹,
232 suggests that also the release of nitrogen oxide or nitric acid takes place. The thermal degradation of
233 nitrate salts, generally proceeds through dehydration followed by the emission of N₂O₅ (or of a gas
234 mixture composed by NO₂ and O₂ in a molar ratio 4:1) [45]. However, in some cases an initial
235 release of nitric acid was recorded [46]. Therefore, the presence of noise makes difficult to
236 distinguish between nitrogen oxide or nitric acid, whereas the temperature suggests that the signals
237 are due to the development of nitric acid. The intensities of signals attributed to ethanol increase in
238 the FTIR spectrum recorded at 223°C (Fig. 4), and the strong band at 1740 cm⁻¹ can be ascribed to
239 the stretching of C=O of acetaldehyde. Pyrolysis of ethanol can proceed through two alternative
240 mechanisms: dehydration with formation of ethylene and water, or dehydrogenation leading to the
241 formation of acetaldehyde and hydrogen (undetectable by FTIR) [47]. The presence of the bands at
242 2800 cm⁻¹ and 2700 cm⁻¹, typical of the C-H vibrations in the aldehyde groups [48], confirms the
243 presence of acetaldehyde. In the spectrum recorded at 263°C the signal of ethanol, CO, CO₂ and
244 acetaldehyde are still evident. In addition, the weak sharp band at 948 cm⁻¹ can be due to the
245 formation of ethylene. The intensity of this signal (as well as that of CO₂) increases in the spectrum
246 recorded at 309°C, whereas only some residue of ethanol and acetaldehyde are detectable

247 suggesting that their degradation is still occurring. The spectrum recorded at 422°C shows only the
248 strong doublets of CO₂ and NO₂ suggesting that the degradation of all organic matter and nitrate
249 ions was completed. At 533°C NO₂ evolves as end-product of nitrate degradation, whereas the low
250 amount of CO₂ is due to the degradation process of calcium carbonate [43].

251 The thermal behaviour of Z90HAp10 is very similar to that of pure ZrO₂ (Z). In the FTIR spectra at
252 95°C and 144°C the sample release only adsorbed water and propanol. The thermal decomposition
253 of the acetylacetone leads to the formation of acetone, CO and CO₂ (in the spectrum at 198°C
254 signals were found at 1745 cm⁻¹, 1220 cm⁻¹-and 1365 cm⁻¹, respectively), whereas only a residue of
255 propanol is still visible as a weak band at 1065 cm⁻¹. Moreover, the sharp band at 948 cm⁻¹ suggests
256 that also the degradation of ethanol takes place leading to the formation of ethylene. The
257 contemporary presence of the zirconia and HAp phases in this material induces a shift toward
258 higher values of the degradation temperature of acetylacetone, in comparison with that of pure
259 zirconia (115°C), and a decrease of the ethanol degradation temperature with respect to that of pure
260 HAp (263°C). Therefore, the degradation phenomena take place at the same temperature (198°C),
261 leading to a strong exothermic effect and the evolution of high amount of gas species that caused
262 the ejection of mass from the crucible during the experiment. At 554°C the degradation of all
263 organic matter was completed and only the band of CO and CO₂ are visible.

264 The first two FTIR spectra of Z70HAp30 collected at 128 and 166°C (Fig. 4), show the release of
265 adsorbed water. At 166°C also CO and CO₂ were detected, suggesting that at this temperature in
266 this sample the partial combustion of organic matter occurs as well as in pure HAp. In the spectrum
267 collected at 248 °C the degradation of the nitrate ions leads to the formation of the typical signal of
268 nitrogen oxides [46].

269 Moreover, an increase of the CO₂ release is shown, due to the degradation of organic matter. At this
270 temperature, also in this sample a weak explosion occurred, probably caused by the overlapping of
271 more exothermic degradation phenomena accompanied by the release of significant amount of gas
272 species. The gas mixture collected at 563°C contains only a residue of CO₂ and the duplet

273 ascribable to the formation of NO_2 , suggesting that the degradation processes of organic matter and
274 of nitrate ions are completed in this temperature conditions.

275 The thermal behaviour and the degradation mechanisms of Z50HAp50 is more similar to those of
276 pure HAp with respect to those of pure ZrO_2 , producing some of the gas species observed for the
277 former, even though they were released at different temperature. The first evolution of gas was
278 observed at lower temperature than for pure HAp (90°C) and corresponds to water and CO_2 .
279 Therefore, the recorded spectrum is very similar to background. Also the presence of the stretching
280 band of $\text{N}=\text{O}$ due to the gas species produced by the degradation of nitrate ions, was found in the
281 spectrum at 160°C , which is lower than that for pure HAp, and in that at 188°C . The spectrum at
282 247°C reveals the development of ethyl phosphate, produced by the reaction of ethanol with P_2O_5
283 [49], leading to consumption of ethanol that could explain its absence in the spectrum. Moreover, its
284 formation delays the evolution of heat due to the alcohol degradation. Therefore, a release of a
285 lower amount of energy occurred, thus avoiding explosive phenomena. The spectrum at 303°C
286 reveals the presence of ethylene, which could be due to the degradation of the ethyl phosphate [50].
287 Finally, NO_2 and CO_2 were detected from the spectrum at 561°C , formed at the end of nitrate
288 degradation and decomposition of calcium carbonate. The release of CO_2 is confirmed also in the
289 spectrum at 667°C , as final thermal degradation product of all the organic molecules and carbonate.
290 Fig. 5 shows the FTIR spectra of the gas mixture evolved during the TG experiments of all the
291 samples treated at 120°C . This post-synthesis treatment leads to the removal of a part of the
292 solvents. Therefore, apart from this low temperature process, the degradation products seem to be
293 the same of fresh samples, thus suggesting that the thermal degradation occurring in those samples
294 follow the same mechanisms described for the untreated samples. However, the evolution of the
295 gaseous species for samples treated at 120°C takes place, in some cases, at temperatures slightly
296 higher than those of fresh ones.

297 Therefore, the obtained results show that in all samples the complete degradation of the organic
298 matter and nitrate ions require heating up to about 600°C . A post-synthesis heat treatment of the

299 gels at lower temperature, thus, could be inadequate to prepare materials potentially suitable to be
300 used as biomaterials, because the absence of toxic by-products is an essential requirement prior of
301 their use.

302

303 *XRD structural study of the composite materials treated at 600 and 1200°C*

304 The XRD spectra of the composite materials investigated (Z90HAp10, 70HAp30, Z50HAp50)
305 pretreated at 120°C revealed that they are amorphous, while those of the samples calcined at 600
306 and 1000°C (including Z and HAp) were reported in Figs. 6 and 7, respectively.

307 As far as the samples treated at 600°C are concerned, Fig. 6a shows the XRD spectrum of pure
308 HAp that does not reveal the presence of calcium phosphate, but only of a small content of calcium
309 oxide. By increasing the amount of Z in the composites (from 50 to 90 mol%) in Fig.6b-d the
310 degree of crystallinity decreases: Z90HAp10 is substantially amorphous, even if treated at 600°C),
311 while Z is found to be present as a mixture of monoclinic and tetragonal phases (*t*-ZrO₂ and *m*-
312 ZrO₂, respectively, in Fig. 6e), with an evident broadening of peaks that suggests the low degree of
313 crystallinity for both phases.

314 As expected, the XRD spectra of the samples treated at 1000°C revealed in Fig. 7 an increase of the
315 degree of crystallinity accompanied by well-defined peaks in almost all the spectra (except for plot
316 d, related to Z90HAp10). Several crystalline phases have been identified in Fig. 7a, whose main
317 ones are hydroxyapatite and calcium phosphate [51], along with small amount of calcium oxide
318 [52]. Similarly to what observed for the composite materials treated at 600°C, also for those treated
319 at 1000°C it is evident that crystallinity decreases with increasing the content of Z, being the
320 intensities and the sharpness of peaks in plot d (related to Z90HAp10) significantly smoothed. Z
321 treated at 1000 (Fig. 7e) is crystallized in the monoclinic system.

322 Two important concluding remarks can be drawn regarding the structural study. First, pure Z
323 crystallizes at 1000°C in one phase (monoclinic one), but the presence of HAp, as a composite
324 material, enables the crystallization in the tetragonal phase. Second, the increasing content of Z

325 causes an increase in the amorphization degree of all the HAp-based composites treated at 600 and
326 1000°.

327 The observed structural modifications are in agreement with the results obtained on the same
328 materials by FTIR spectroscopy in a previous recent study [30], and affect remarkably the
329 biological properties of the investigated materials. The material heated at 1000°C showed higher
330 biocompatibility, explained previously in terms of an higher ability to absorb blood protein for the
331 cell adhesion [30]. This ability is influenced by the release of ions from these materials [53], which
332 affects the surface charge and, in turn, is affected by the crystallization degree [31].

333

334

335 **Conclusion**

336 The thermal behavior of pure zirconia, hydroxyapatite and of three zirconia/hydroxyapatite
337 composite materials has been investigated under inert atmosphere by TG coupled by FTIR to
338 analyze the gases evolved during the occurrence of each thermally stimulated process. Moreover,
339 the structural modification of the samples caused by the thermal treatment was investigated by
340 XRD. The results obtained in the present study allow identifying the temperatures able to induce
341 specific degradation phenomena or structural reorganization, that are essential information to
342 develop a materials potentially suitable to be used as biomaterials. The correlation of those data
343 with the known biological performances showed by the same ZrO₂/HAp composites as a function
344 of the post-synthesis heat-treatment, along with further information (e.g. identification of the ions
345 released from the materials, of the activated biochemical pathways, of the induced cell cycle
346 alteration, etc.) could be a useful tools to explain the mechanisms driving the biological response to
347 these materials.

348

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499 **Captions of the figures**

500

501 **Fig. 1.** TG/DTG curves at 10 K min^{-1} under a nitrogen purging gas atmosphere of fresh (not
502 thermally treated) materials.

503

504 **Fig. 2.** Sample temperature vs. time plots of TG experiments for: Z90HAp10 (a-c); Z70HAp30 (d-
505 f).

506

507 **Fig. 3.** TG/DTG curves at 10 K min^{-1} under a nitrogen purging gas atmosphere of materials treated
508 at 120°C .

509

510 **Fig. 4.** FTIR spectra of the gas mixture evolved during TG analysis at different temperatures for
511 fresh (not thermally treated) materials.

512

513 **Fig. 5.** FTIR spectra of the gas mixture evolved during TG analysis at different temperatures for
514 materials treated at 120°C .

515

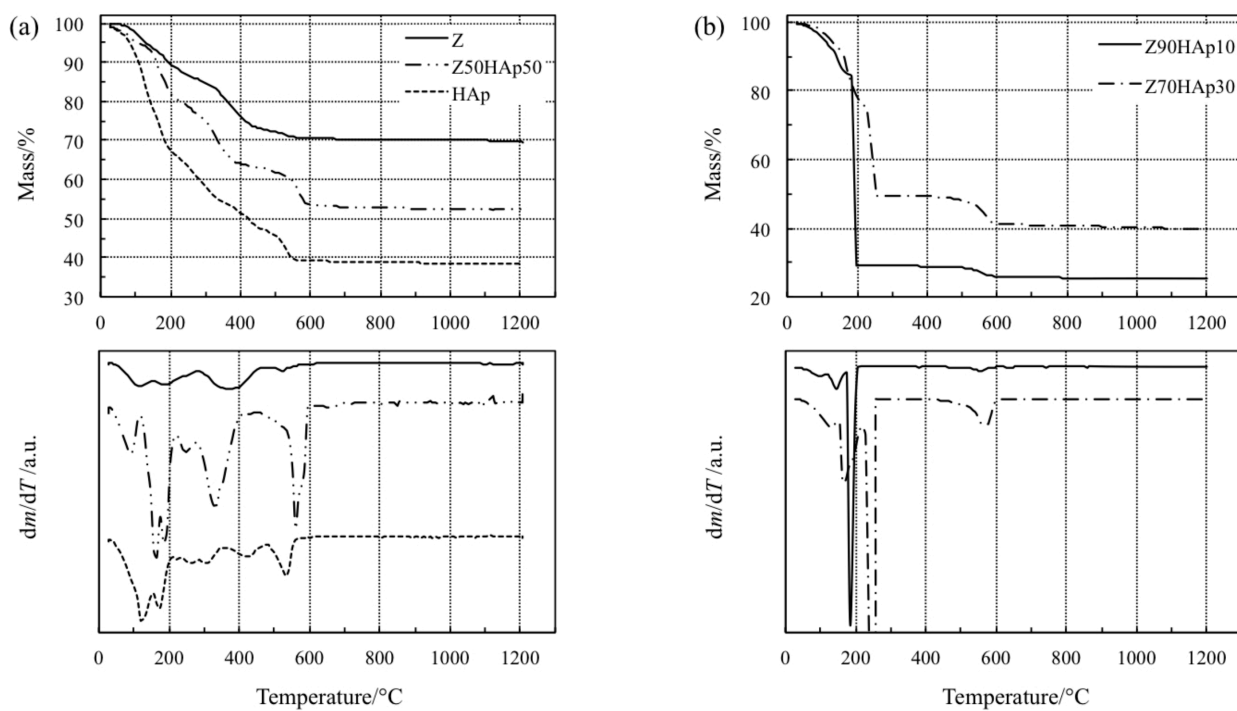
516 **Fig. 6.** X-ray diffraction pattern of materials treated at 600°C : Z (a), Z90HAp10 (b); Z70HAp30
517 (c); Z50HAp50 (d); HAp (e). Phases identified: hydroxyapatite (\star), $t\text{-ZrO}_2$ ($\#$), $m\text{-ZrO}_2$ ($^\circ$), calcium
518 phosphate (+) and calcium oxide (\wedge).

519

520 **Fig. 7.** X-ray diffraction pattern of materials treated at 1000°C : Z (a), Z90HAp10 (b); Z70HAp30
521 (c); Z50HAp50 (d); HAp (e). Phases identified: hydroxyapatite (\star), $t\text{-ZrO}_2$ ($\#$), $m\text{-ZrO}_2$ ($^\circ$), calcium
522 phosphate (+) and calcium oxide (\wedge).

523 Fig. 1

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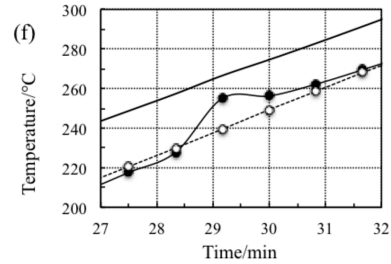
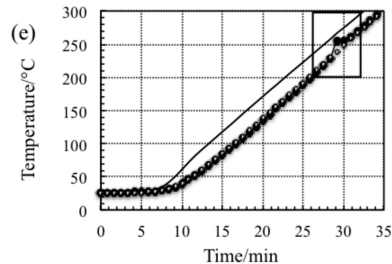
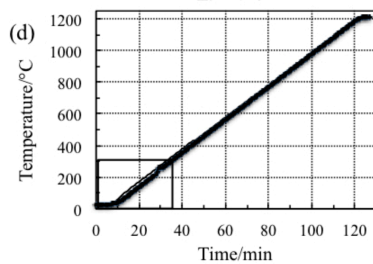
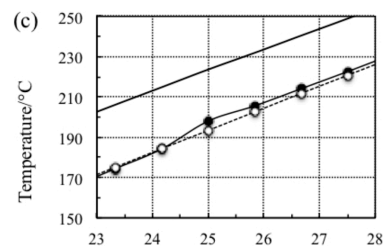
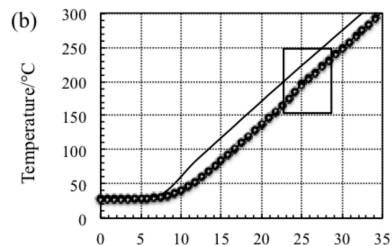
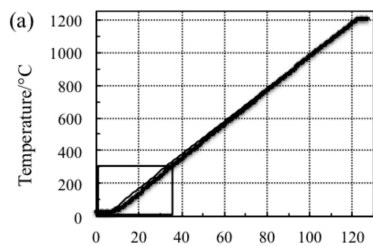
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528 Fig. 2

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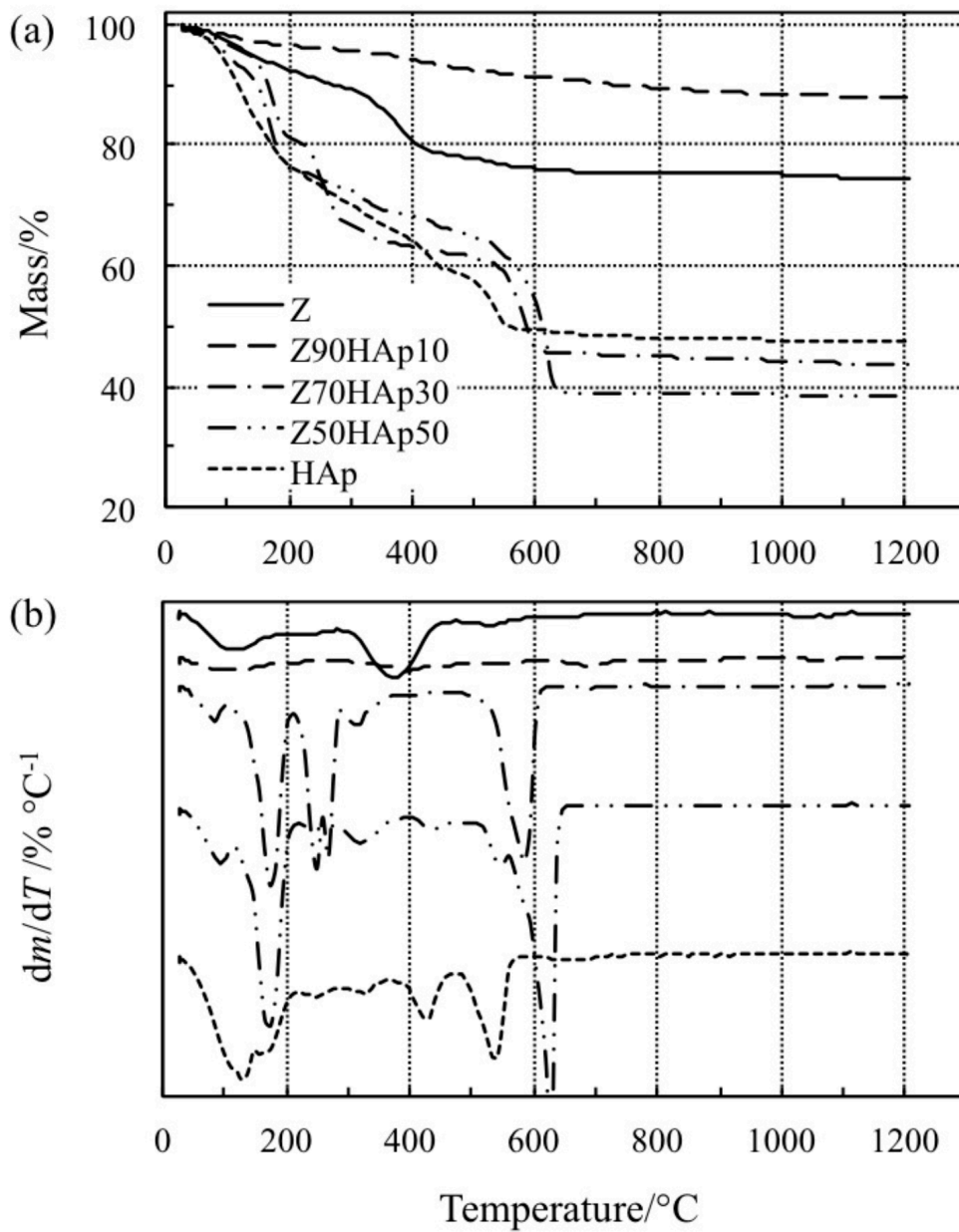
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534 Fig. 3

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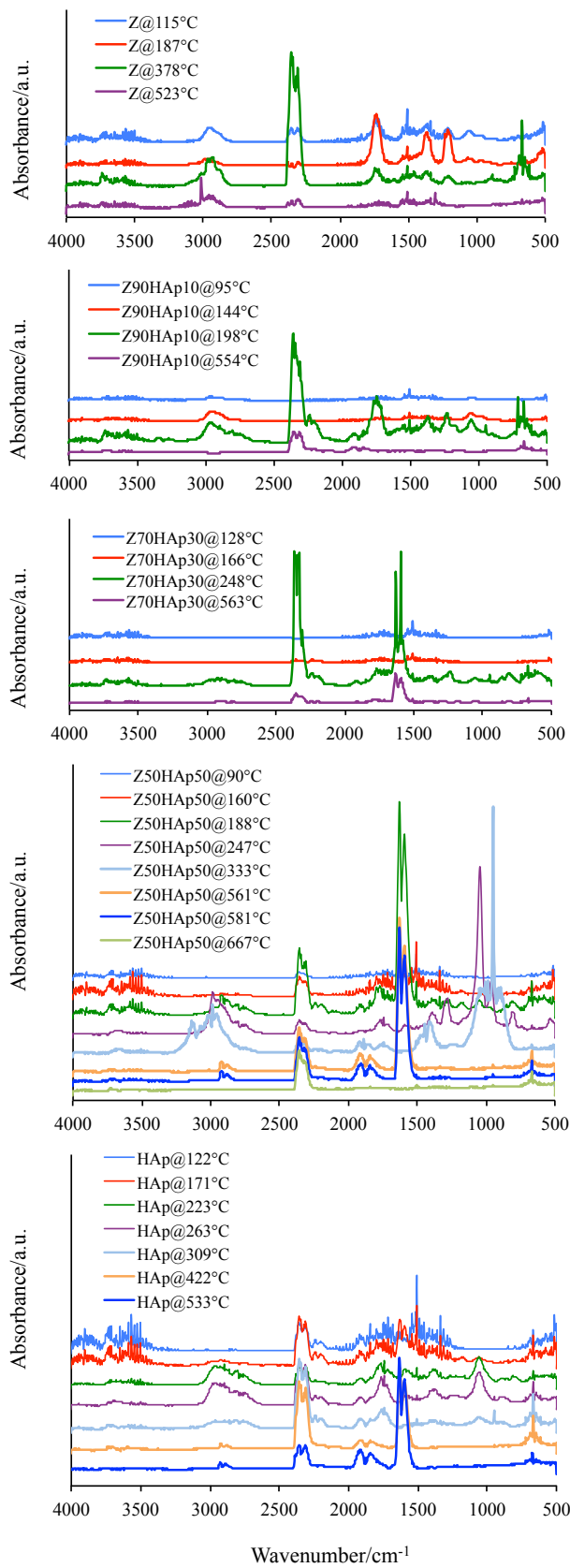
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540 Fig. 4

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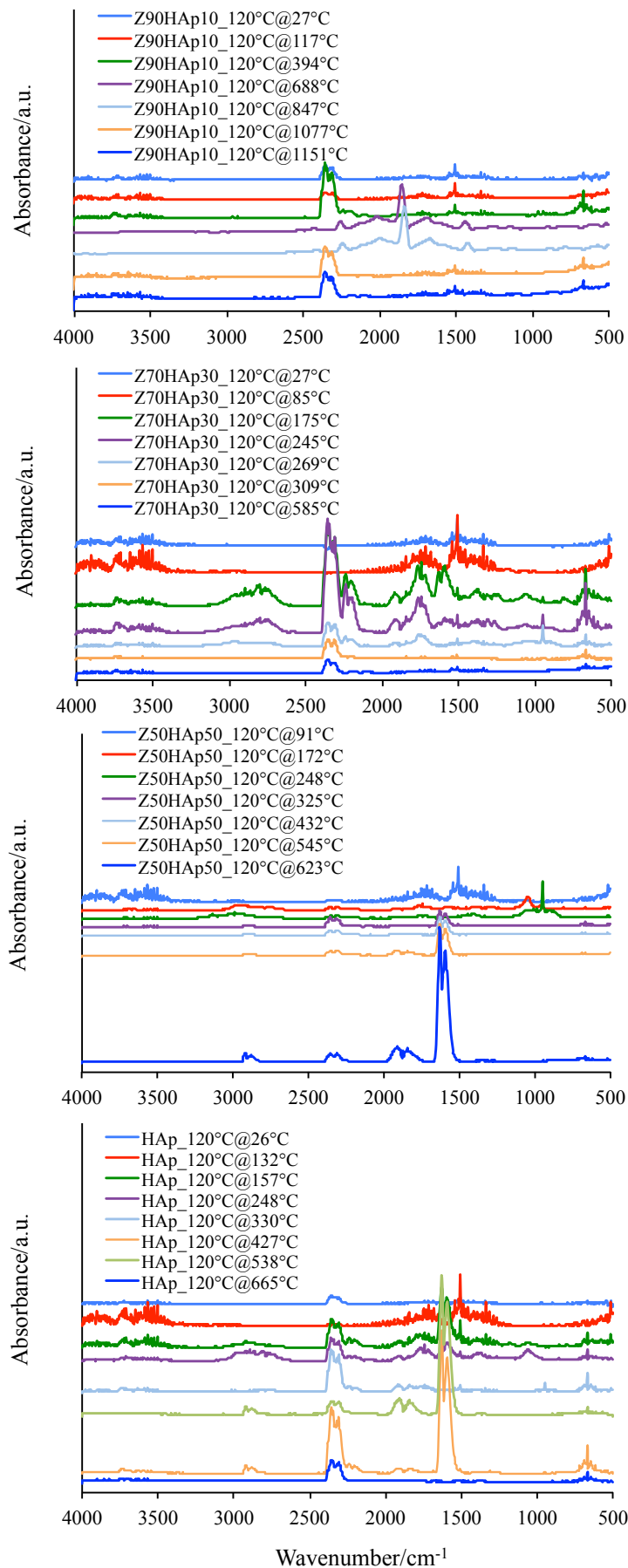
544 Fig. 5

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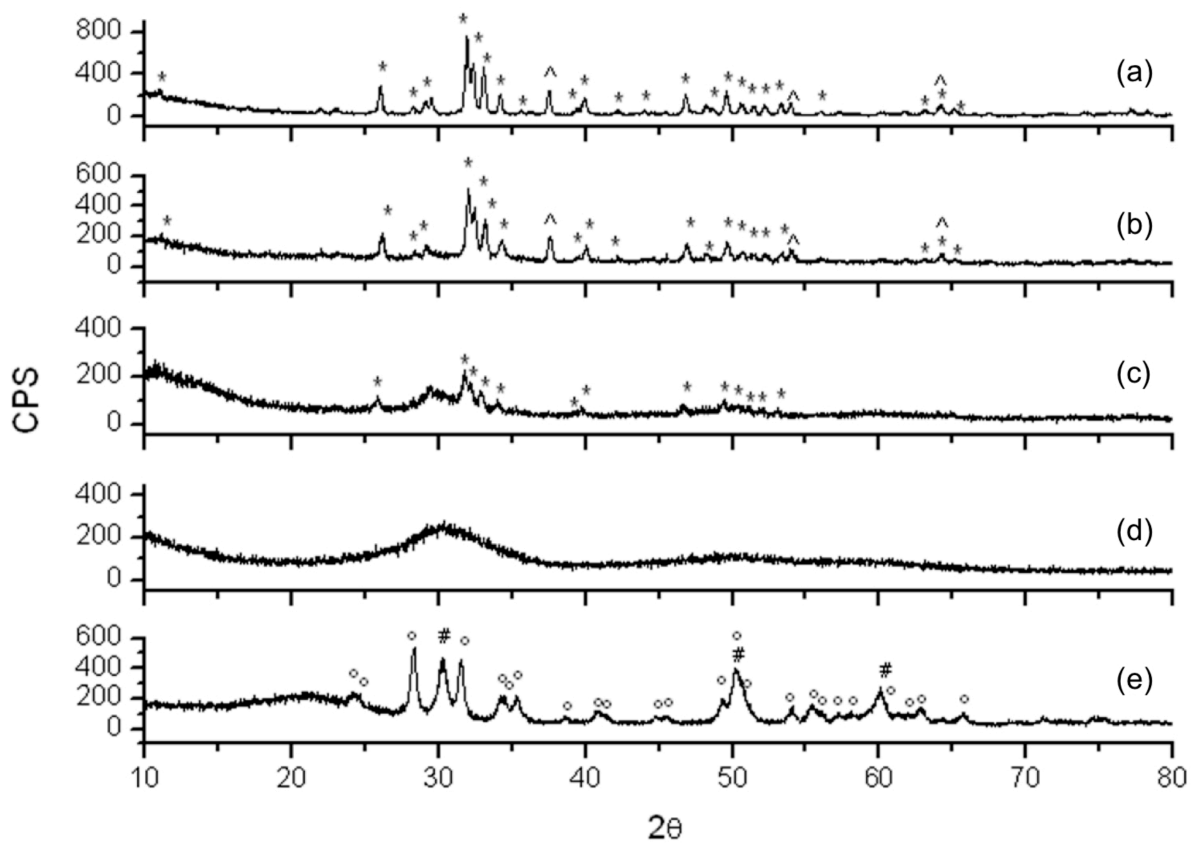
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549 Fig. 6

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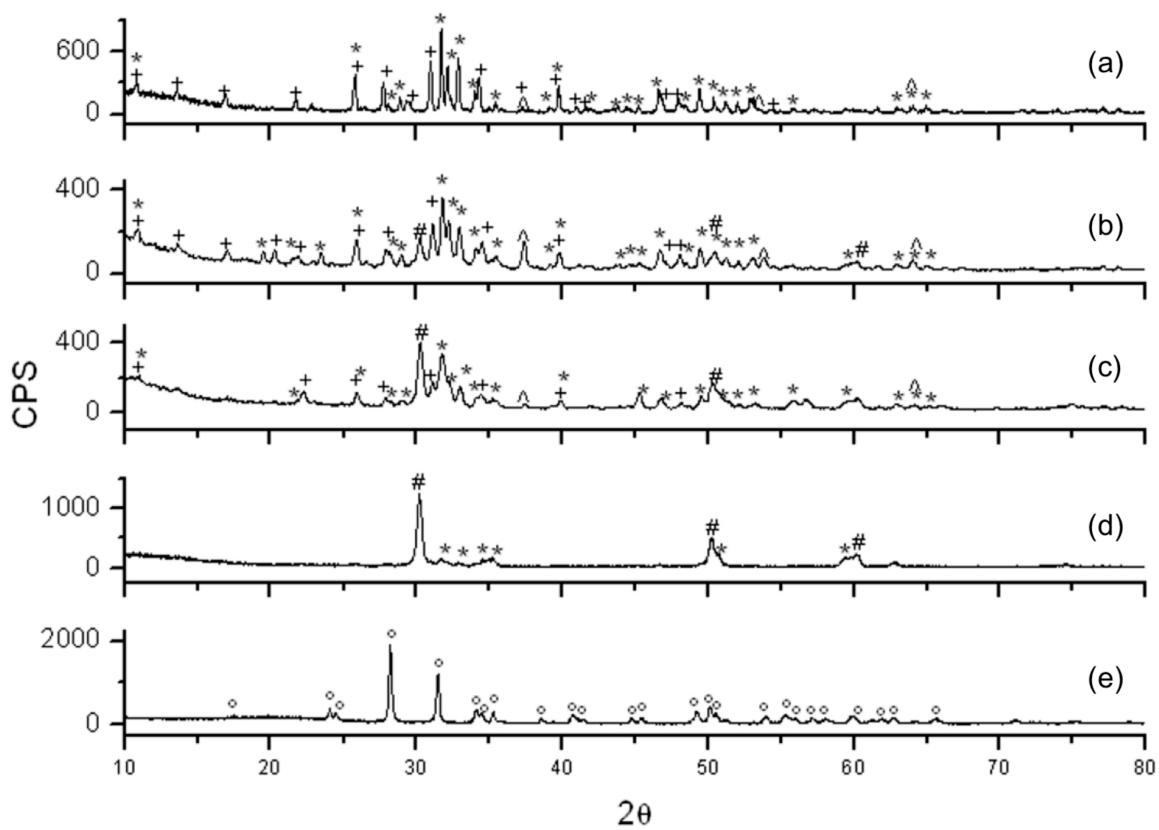
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555 Fig. 7

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